

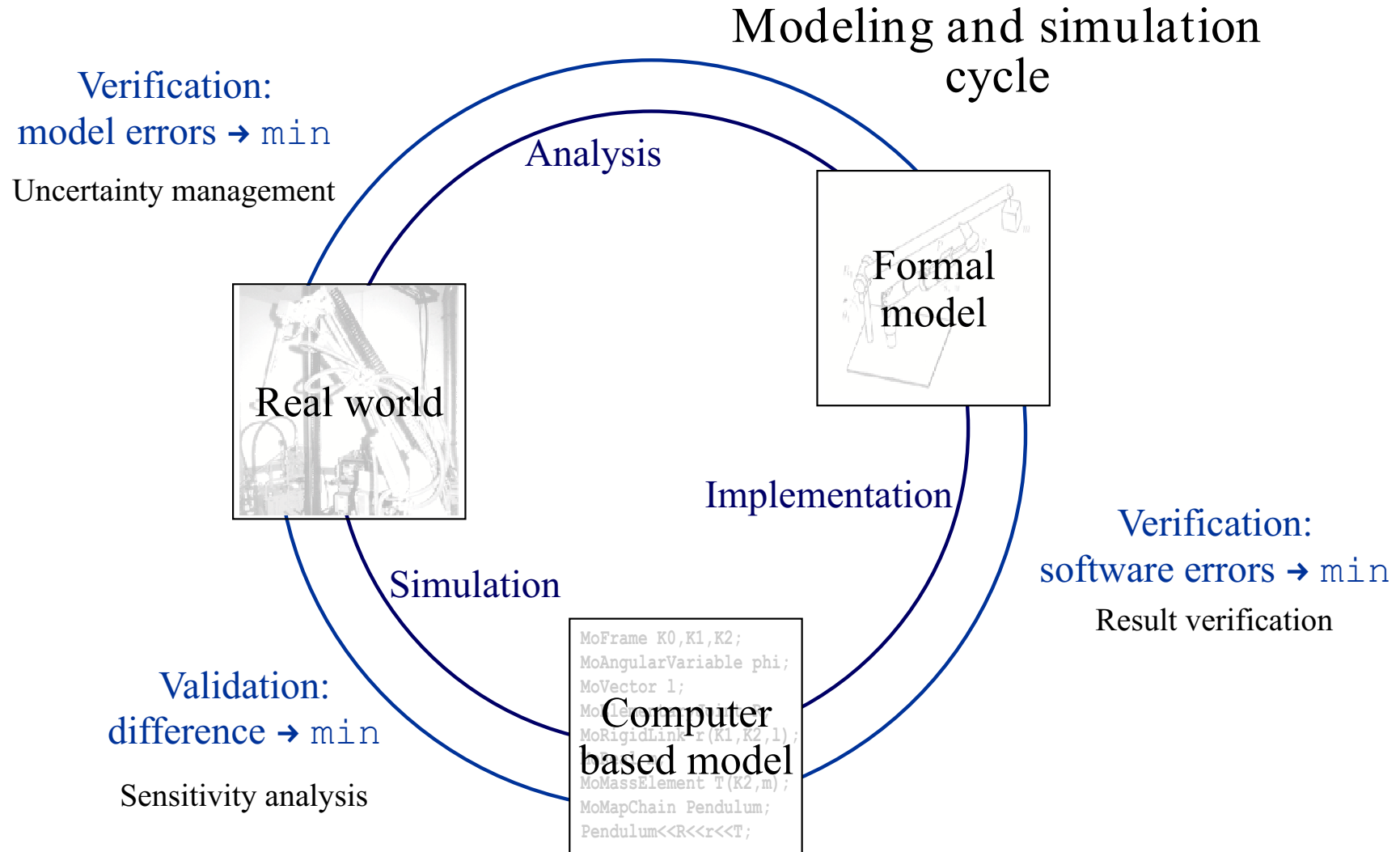
Verification and Validation of Two Biomechanical Problems

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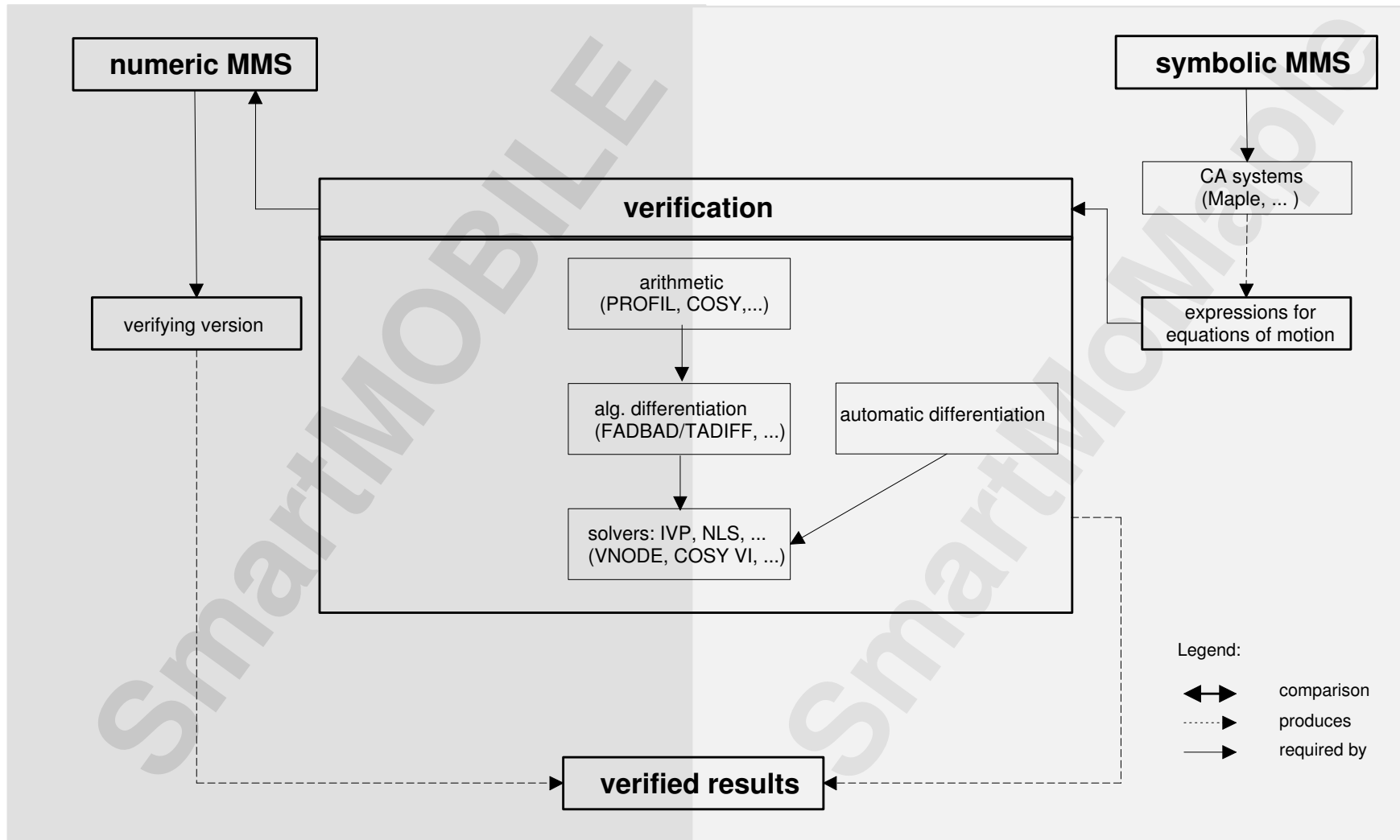
University of Duisburg-Essen, Germany

SCAN, September-October 2008

1 Motivation



Approaches



SMARTMOBILE / SMARTMOMAPLE —

Simulation and Modeling of dynAmics: **R**eliable and **T**emplate-based/ au**T**omatized

Applications in Biomechanics

Find out how changes in parameters influence the result

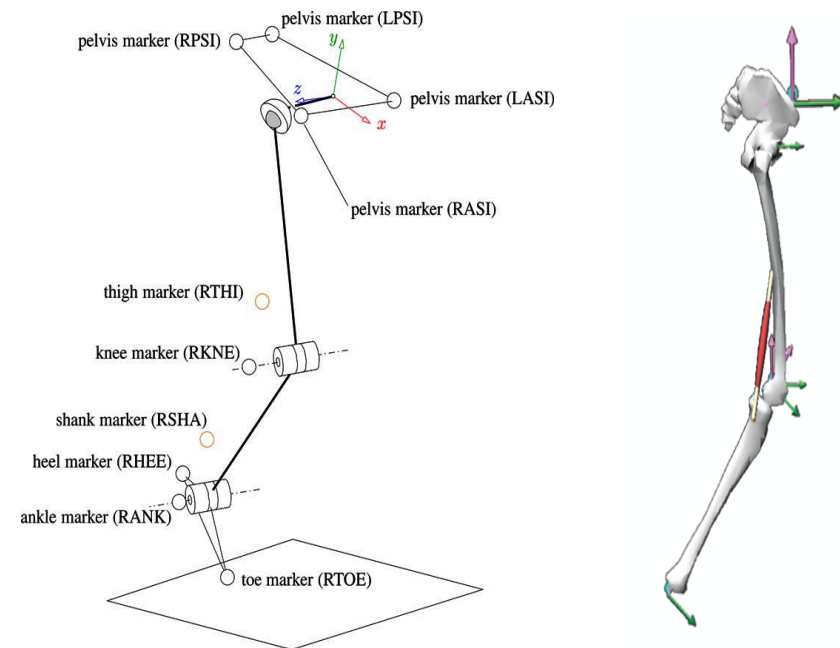
1. Identification of body segment motion

- quantify the influence of marker displacements on motion

2. Muscle activation model

- find the sensitivity of the model to its parameters
- work with piecewise (differentiable) functions

3. Many more...



Topics

- Theoretical aspects
- Main features of SMARTMOBILE and SMARTMOMAPLE
- Identification of body segment motion
- A simplified muscle activation model
- Conclusions

2 Theory: Important Concepts and Facts

Arithmetics Intervals, Taylor models

Solvers Pure iteration: need Jacobians or rely on their arithmetic
 Series based: need e.g. Taylor coefficients and their Jacobians

AD Code transformation, **overloading**

Sensitivity Definition: $s = \frac{\partial[x]}{\partial[p]}$, where $[p]$ is an (uncertain) parameter
 Meaning: a linear measure of uncertainty influence
 Reference: $s = \frac{\partial x}{\partial p} \times \text{uncertainty}(p)$ with intervals

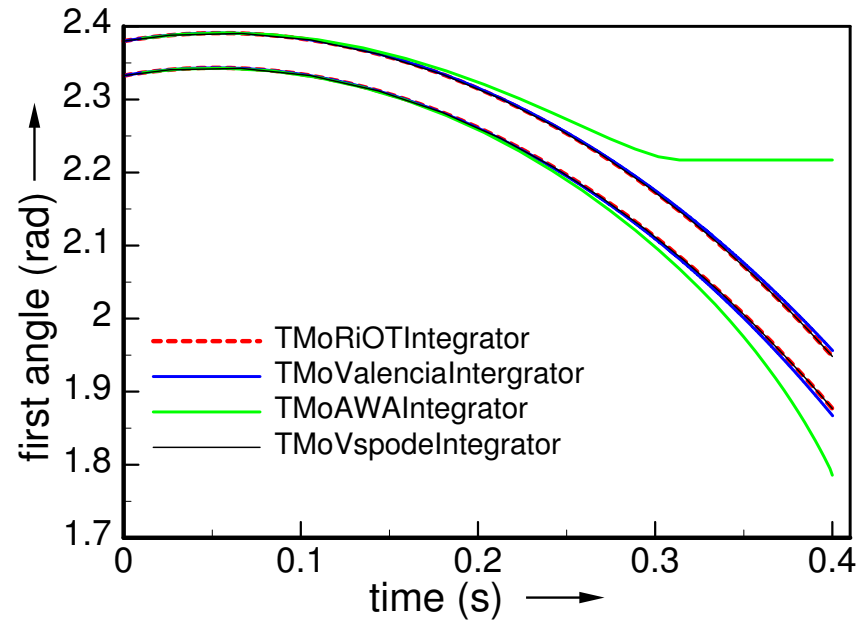
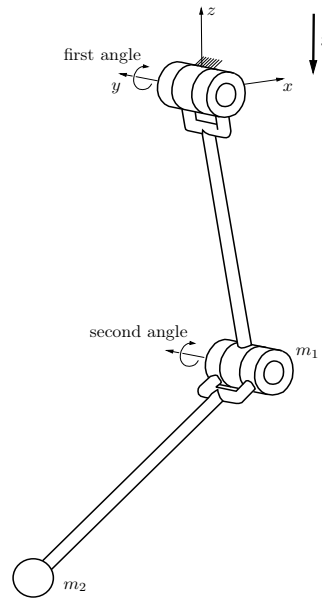
4 Main Features of SMARTMOBILE

1. Based on MOBILE by A. Kecskeméthy
2. Verified kinematics/dynamics + uncertainty management
3. Free choice of the underlying arithmetic: templates + solvers

Type	Integrator	Purpose
MoReal	MoAdams, ...	nonverified dynamics
TMoInterval	TMoAWA	verified dynamics of ODE based systems
TMoFInterval	TMoValencia	
TMoTaylorModel	TMoRiOT	
TMoTaylorModel	TMoVSPODE	
RDAInterval	---	Taylor model based kinematics
MoFInterval	MoIGradient	verified equilibria kinematics with constraints
MoSInterval	TMoValenciaS	verified sensitivity

4. Converters MOBILE \longrightarrow SMARTMOBILE

Example: Dynamics of a Double Pendulum with an Uncertain Initial Angle



```
# define TMoInterval t;
TMoFrame<t> K0, K1, K2, K3, K4;
TMoAngularVariable<t> psi1, psi2;
// transmission elements
TMoVector<t> l1(0,0,-1), l2(0,0,-1);
TMoElementaryJoint<t> R1(K0,K1,psi1,xAxis);
TMoElementaryJoint<t> R2(K2,K3,psi2,xAxis);
TMoRigidLink<t> rod1(K1,K2,l1),rod2(K3,K4,l2);
t m1(1),m2(1);
TMoMassElement<t> Tip1(K2,m1),Tip2(K4,m2);
// the complete system
TMoMapChain<t> Pend;
Pend << R1<<rod1<<Tip1<<R2<<rod2<<Tip2;
// dynamics
TMoVariableList<t> q; q << psi1<<psi2;
TMoMechanicalSystem<t> S(q,Pend,K0,zAxis);
TMoAWAIntegrator I(S,0.0001,ITS_QR,15);
I.doMotion();
```

Strategy	TMoAWA (variable h)	TMoRiOT ($0.0002 \leq h \leq 0.2$)	TMoValencia ($h = 10^{-4}$)	TMoVSPODE (variable h)
Break-down	0.420	0.801	0.531	0.656
CPU Time*	5	285	22	10

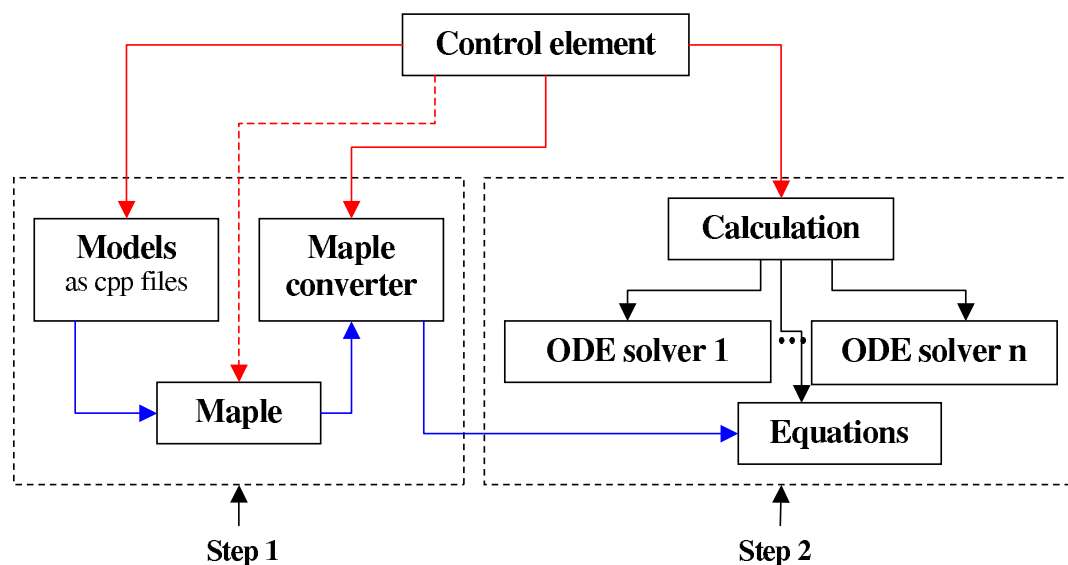
* computed on $8 \times$ Intel Xeon CPU 2.00GHz under Linux 2.6.25.14-69.fc8

5 SMARTMOMAPLE – Symbolic Counterpart to SMARTMOBILE

MOMAPLE

- a package for MOBILE
- creates *symbolic* expressions via MAPLE
- no closed loop systems
- modeling only, simulation not automatized

SMARTMOMAPLE*



- automatizes symbolic simulations
- semi-automatic integration of (verified) ODE solvers possible
- currently available: VNODE-LP, RIOT, VALENCIA-IVP

* Inna Reinke, Master thesis, October 2008

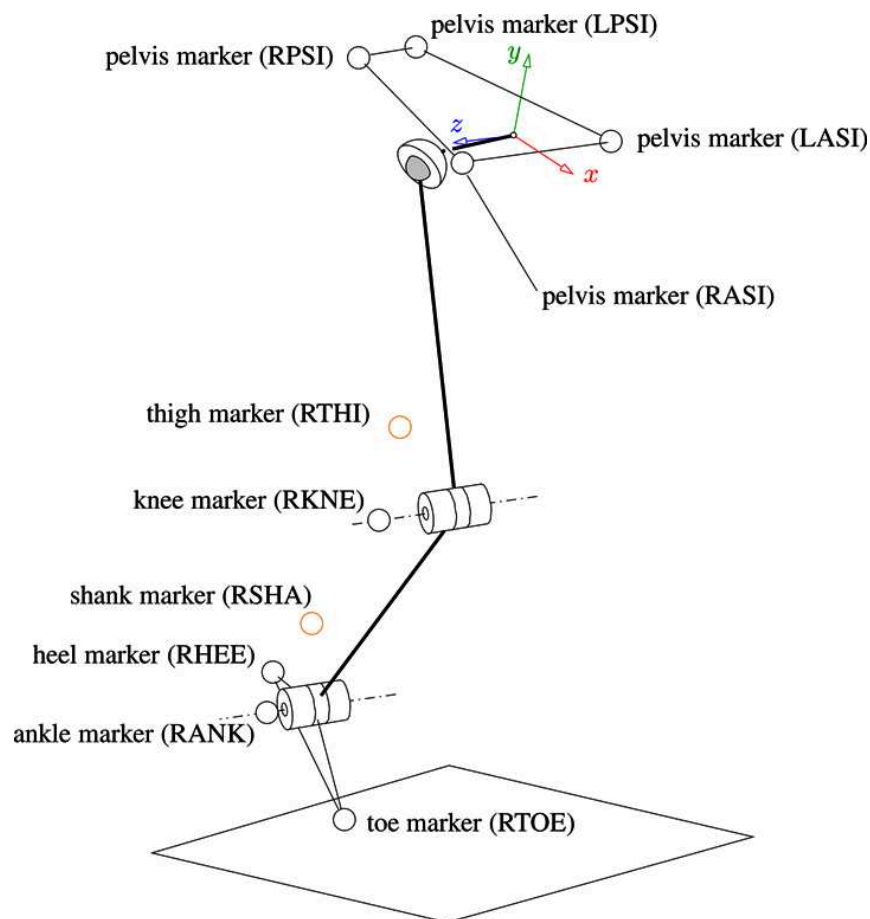
Example: Dynamics of a Double Pendulum in SMARTMOMAPLE

(numbers in this color show data from SMARTMOBILE)

Strategy	VNODE-LP (variable h)		RiOT ($0.0002 \leq h \leq 0.2$)		VALENCIA-IVP ($h = 10^{-4}$)	
Break-down	0.520	0.420	> 2	0.801	0.606	0.531
CPU Time	6	5	80min	285	106	22

SMARTMOMAPLE: – slower for this example
– later breakdown

6 Identification of Body Segment Motion



Parameters (mm):

knee width	120 ± 10
ankle width	80 ± 10
displacements	tangential/soft tissue ± 10 normal ± 5

Femur length (mm):

	TMoRDA	INTERVAL
Knee, ankle	[377.6; 396.7]	[0; ∞]
Skin displacement	[0.000; 621.4]	no answer

Sensitivity of femur wrt.

Knee	Ankle	Tangential	Normal	Soft
0.4	-0.3	-2	0.7	1.4

$\pm 7\text{mm}$

$\pm 37.5\text{mm}$

Reference uncertainty:

7 A Simplified Muscle Activation Model

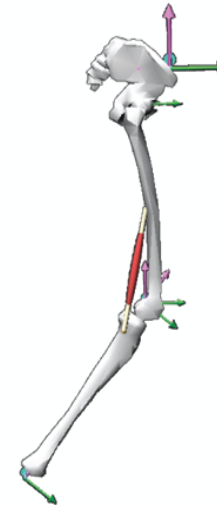
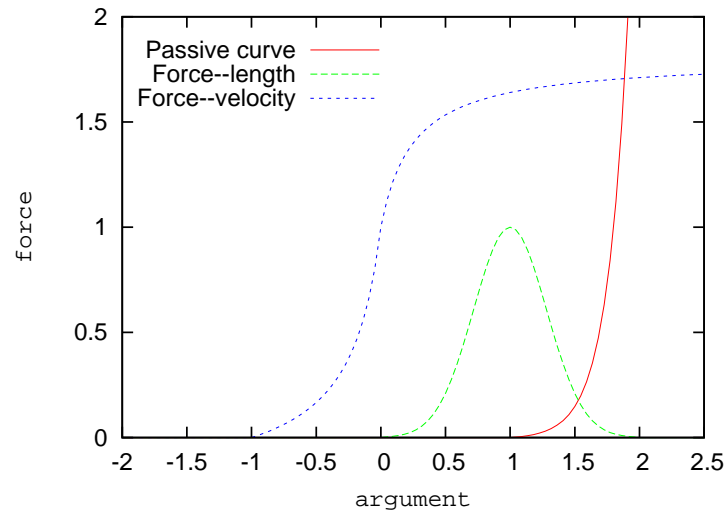
Model Description*

The Hill type muscle model:

$$F = F_{max} F_P(l) + F_{max} a(t) F_L(l) F_H(v)$$

Simplified for verification:

PT muscle model



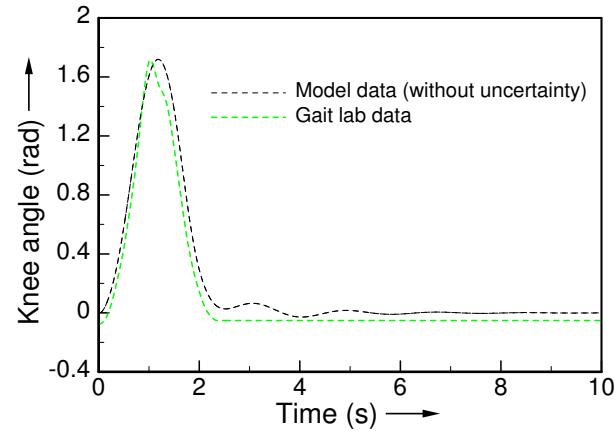
$$F(s) = \frac{P}{1 + Ts}$$

$a(t)$: linear equidistant piecewise and exponential camel-back

$a(t)$: exponential camel-back

* D. Strobach et al., *A simplified approach for rough identification of muscle activation profiles via optimization and smooth profile patches*,

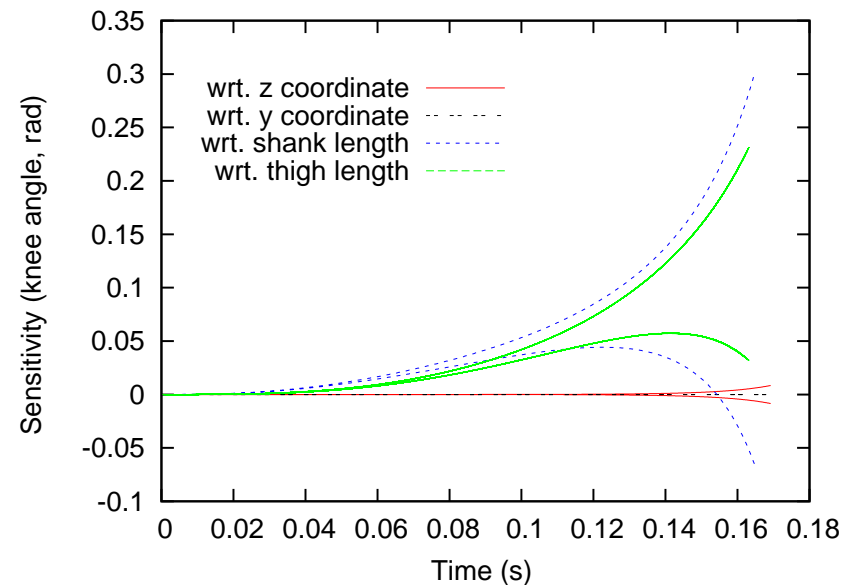
Verified Simulation in SMARTMOBILE (PT Muscle Model)



Uncertainty ($\pm 0.1\%$)	Break down
Thigh length = 0.45	0.118
Shank length = 0.49	0.125
$z = -0.2281$	0.135
$y = -0.0253$	0.389

Sensitivities under $\pm 0.1\%$ uncertainty in

- thigh and shank lengths
- muscle insertion points
- z coordinate
- y coordinate



8 Towards Working With Piecewise Functions

Necessary: AD for `if` operator

Provided by: CPPAD — template based AD library (`double`)

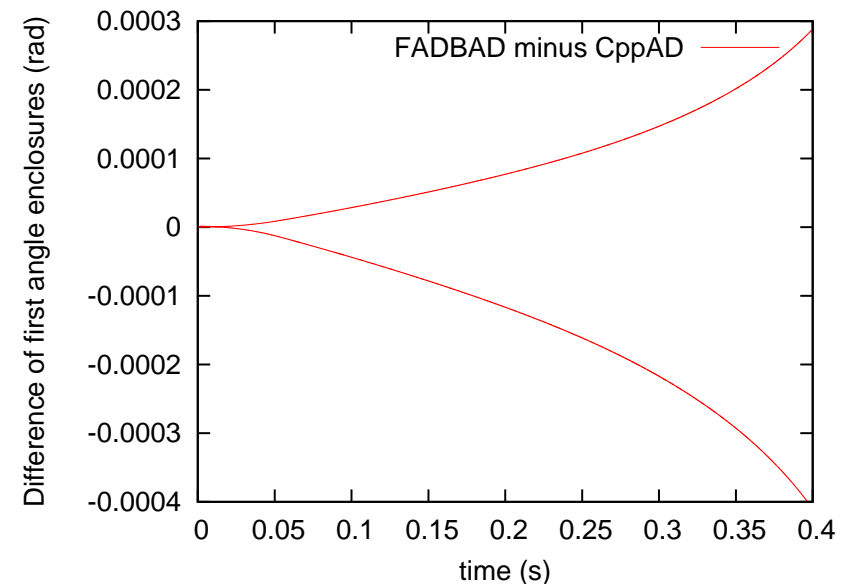
Comparison: The Double Pendulum with CPPAD (1) and FADBAD (2)

Kinematics:

		$\partial y / \partial \beta_1$	$\partial y / \partial \beta_2$	CPU (<i>ms</i>)
double	(1)	0.1011	0.8082	0.106
	(2)	0.1011	0.8082	0.118
INTERVAL	(1)	[0.0705,0.1317]	[0.7513,0.8647]	0.400
	(2)	[0.0661,0.1360]	[0.7513,0.8647]	0.300

β_1 for double = Mid($[\beta_1]$)

Dynamics with VALENCIA:



CPU: 36s for (1), 22s for (2)

Kinematics with Piecewise Differentiable Functions

Hill type muscle model: Find sensitivity of the knee position to $\pm 1\%$ uncertainty in the thigh length $p = 0.45\text{m}$

	x	z	$\partial x / \partial p$	$\partial z / \partial p$
double	0.226	0.514	-0.033	-0.9995
INTERVAL	[0.222, 0.231]	[0.509, 0.519]	-[0.032, 0.033]	-[0.9994, 0.9995]

Reference uncertainty: $\pm 1\text{mm}$ in x , $\pm 2.3\text{mm}$ in z

Vastus intermedius

with $l_i = [0.809, 1.199]$,

$l_d = 1.001$

	double	INTERVAL
passive curve	$4.938e - 05$	$[-0.004, 0.001]$
force-length	0.999992	$[0.782, 1.000]$
force-velocity	not used	not used

Piecewise Functions For Intervals

Difficulty:	Comparison operators for intervals
Comparison:	if (a<b) x=x1 else x=x2 , where <i>a</i> interval, <i>b</i> point interval
CPPAD syntax:	x=CondExpLt(a,b,x1,x2)
a<b for double:	yes or no
CondExpLt for double:	double CondExpLt(a, b, x1, x2){ if(a<b) return x1; else return x2; }
a<b for INTERVAL:	inclusion or <i>yes/no/possibly</i>
CondExpLt for INTERVAL:	INTERVAL CondExpLt(a, b, x1, x2){ if(Sup(a)<Inf(b)) return x1; else if(Inf(a)>Sup(b)) return x2; else return x3=f(a,b,x1,x2)=?; }

Choices for $f(a, b, x1, x2)$

Possibility 1: Externally through $x = \text{CondExpLt}(a, b, x1, x2, \text{maybeCase})$, where $\text{maybeCase} := f$ (not supported in CPPAD)

Possibility 2: Construct from $x1$ and $x2$

But:

- $x1, x2$ intervals, not functions of x
- Unknown function values in b
- No knowledge about if a, b are function or argument values
- No general strategy possible without extra knowledge

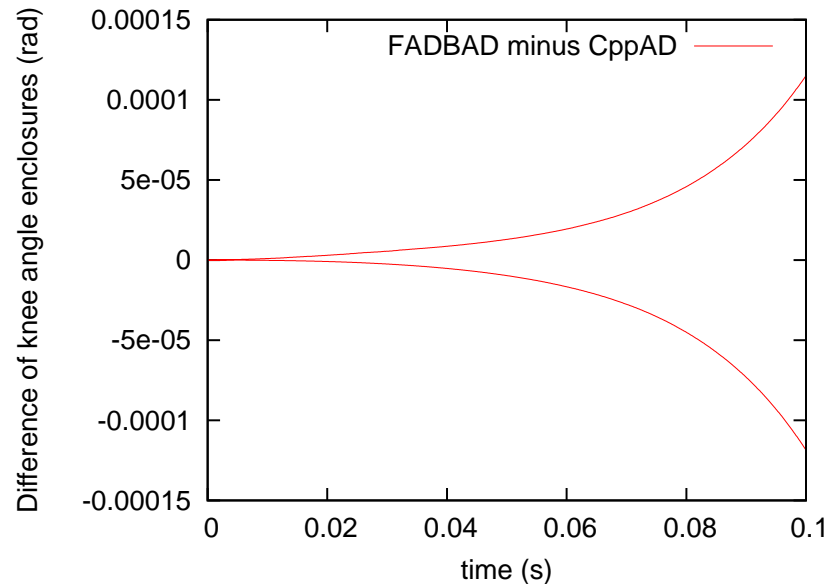
Solution: A special comparison operator, preferably without disjoint intervals?

Dynamics With Simple Piecewise Functions (PT Muscle Model)

Physical constraints for

activation: $0 \leq a(t) \leq 1$

force of the PT muscle: $F \leq 0$



Comparison operator:

$$f(a, b, x1, x2) =$$

$$\text{Hull}(\text{Inf}(x1), \text{Sup}(x2))$$

Function values are compared!

Unfortunately, no improvement in break down times for this model!

9 Conclusions

- Segment motion:**
- overestimation reduced through Taylor models
 - reference uncertainty is considerable too
- Muscle activation:**
- sensitivities of the smooth model obtained
 - simple piecewise functions tested for dynamics
 - kinematics for the Hill type muscle model
- Open question:** definition of `if` and `CondExp` for intervals